Clinical Biomechanics

Comparative In Vitro Biomechanical Stiffness Study of A Viscoelastic Disc Versus The Native Lumbar Disc --Manuscript Draft--

Research Paper	
Lumbar Spine; Total Disc Replacement; AxioMed® Viscoelastic Disc; Spinal Biomechanics; Stiffness; In Vitro Testing	
Kingsley R Chin, M.D Less Exposure Surgery Specialists Institute (LESS Institute) HOLLYWOOD, FL UNITED STATES	
Kingsley R Chin, M.D	
Kingsley R Chin, M.D	
Sukanya Chebrolu, MS	
Roger D Sung, MD	
Jeffrey R Carlson, MD	
Mark W McFarland, DO	
Erik Spayde, MD	
William M Costigan, MD	
Sandra Thompson, MD	
Vito Lore, PE	
Kari B Zimmers	
Hope Estevez	
Swapnil Pangarkar	
Aditya Humad	
Chukwunonso C Ilogu, MD	
Jason A Seale, MBBS	
Background Artificial disc replacements aim to preserve motion in patients with lumbar disc degeneration, but most do not replicate the natural stiffness of the healthy human lumbar disc. Existing ball-and-socket designs often permit excessive motion and fail to provide the nonlinear, load-dependent stiffness that is characteristic of native spinal biomechanics. To date, no in vitro study has directly compared the stiffness of a viscoelastic disc implant to that of the natural lumbar disc under physiologic conditions. Methods Ten viscoelastic disc implants were tested using standardized protocols in a physiologic environment (phosphate-buffered saline at 37±3°C). Axial compression, flexion-extension, and axial rotation stiffness were measured using servohydraulic test systems. An additional five implants underwent static axial loading up to 20,000 newtons. All values were compared to published stiffness ranges for the healthy human lumbar disc. Findings	

8

1 Highlights

- Viscoelastic disc implant mimics native lumbar stiffness across key loading modes
- Axial, flexion-extension stiffness matched healthy disc; rotation was more flexible
- Static tests confirmed durability up to 20,000 newtons without mechanical failure
- Load-displacement loops reproduced physiologic neutral and elastic zones
- First in vitro stiffness comparison of viscoelastic disc to native human lumbar disc

```
Title: Comparative In Vitro Biomechanical Stiffness Study of A Viscoelastic Disc Versus The
 1
 2
      Native Lumbar Disc
 3
      Kingsley R Chin MD<sup>1,2,3,4,5</sup>
 4
 5
      Sukanya Chebrolu MS<sup>5</sup>
 6
      Roger D Sung MD<sup>6</sup>
 7
      Jeffrey R Carlson MD<sup>7</sup>
 8
      Mark W McFarland DO<sup>7</sup>
 9
      Erik Spavde MD<sup>8</sup>
10
      William M Costigan MD<sup>9</sup>
      Sandra Thompson MD<sup>10</sup>
11
      Vito Lore<sup>5,11</sup>
12
13
      Kari B Zimmers<sup>12</sup>
14
      Hope Estevez<sup>1,5</sup>
      Swapnil Pangarkar<sup>5</sup>
15
16
      Aditya Humad<sup>5</sup>
      Chukwunonso C Ilogu MD<sup>1,5</sup>
17
      Jason A Seale MBBS<sup>1,5</sup>
18
19
20
       <sup>1</sup>Less Exposure Spine Surgery Institute (LESS Institute aka LESS Clinic), Fort Lauderdale,
21
      Florida, USA; <sup>2</sup>LESS Institute of Jamaica, Kingston, St. Andrew, Jamaica, West Indies;
22
      <sup>3</sup>Department of Orthopedics, Herbert Wertheim College of Medicine at Florida International
      University, Miami, Florida, USA; <sup>4</sup>Faculty of Science and Sports, University of Technology,
23
      Kingston, St. Andrew, Jamaica; <sup>5</sup>Less Exposure Spine Surgery (LESS) Society 501©(3), Fort
24
      Lauderdale, Florida, USA; <sup>6</sup>Colorado Springs Orthopaedic Group, Colorado Springs, CO, USA;
25
       <sup>7</sup>Orthopaedic and Spine Center, Newport News, VA, USA; <sup>8</sup>St. Charles Spine Institute,
26
      Thousand Oaks, CA, USA; 9Congress Orthopaedic Associates, Pasadena, CA, USA; 10The Pain
27
28
      Center, Boise, ID, USA; <sup>11</sup>LESSpine, Burlington, MA, USA; <sup>12</sup>AxioMed LLC, Burlington, MA,
29
      USA.
30
31
      Corresponding Author:
32
      Kingsley R. Chin, MD, MBA
33
      Less Exposure Surgery Specialists Institute (LESS Institute aka LESS Clinic),
34
      6550 N Federal Hwy, Suite 510, Fort Lauderdale, Florida, 33308.
35
      Email: kingsleychin@thelessinstitute.com
36
37
      Conflicts of interest and sources of funding: We did not seek or receive any funding from the
38
      National Institutes of Health (NIH), Wellcome Trust, Howard Hughes Medical Institute (HHMI),
39
      or others for this work. KRC is the cofounder and CEO of Kingsley Investment Company (KIC)
40
      Ventures and has ownership shares in the company. WMC, ST, AH and ES have shares in KIC
41
      Ventures.
42
43
       Word Count:
44
      Abstract: 242
45
      Main Text: 1,804
```

Structured Abstract

2 Background

- 3 Artificial disc replacements aim to preserve motion in patients with lumbar disc degeneration,
- 4 but most do not replicate the natural stiffness of the healthy human lumbar disc. Existing ball-
- 5 and-socket designs often permit excessive motion and fail to provide the nonlinear, load-
- 6 dependent stiffness that is characteristic of native spinal biomechanics. To date, no in vitro study
- 7 has directly compared the stiffness of a viscoelastic disc implant to that of the natural lumbar
- 8 disc under physiologic conditions.
- 9 Methods
- 10 Ten viscoelastic disc implants were tested using standardized protocols in a physiologic
- environment (phosphate-buffered saline at 37 ± 3 °C). Axial compression, flexion-extension, and
- 12 axial rotation stiffness were measured using servohydraulic test systems. An additional five
- implants underwent static axial loading up to 20,000 newtons. All values were compared to
- published stiffness ranges for the healthy human lumbar disc.
- 15 Findings
- Axial stiffness ranged from 1.55 to 3.48 kN/mm, overlapping the reported native range of 0.5 to
- 17 2.5 kN/mm. Flexion-extension stiffness (1.4–2.14 Nm/deg) matched the physiologic range (0.8–
- 18 2.5 Nm/deg). Rotation stiffness (0.72–0.83 Nm/deg) was lower than native values (2.0–9.6
- 19 Nm/deg), resulting in greater rotational mobility. All implants withstood static compression to
- 20 20,000 newtons without structural failure.
- 21 Interpretation
- 22 These findings show that this viscoelastic disc implant more closely reproduces the stiffness of
- 23 the natural lumbar disc than prior designs. The ability to replicate both compliant and stiff

1	loading zones suggests improved biomechanical performance and segmental stability, supporting
2	its use as a potential alternative to spinal fusion.
3	
4	Keywords: Lumbar Spine, Total Disc Replacement, AxioMed® Viscoelastic Disc, Spinal
5	Biomechanics, Stiffness, In Vitro Testing
6	
7	
8	

1 Introduction

- 2 Lumbar degenerative disc disease (DDD) is a major cause of chronic low back pain and
- disability, often requiring surgical intervention when conservative treatments fail. Total disc
- 4 replacement (TDR) has emerged as a motion-preserving alternative to spinal fusion, aiming to
- 5 maintain segmental mobility while alleviating pain [1-3]. However, early-generation articulating
- 6 TDRs have shown limitations in replicating the full biomechanical behavior of the native
- 7 intervertebral disc[4, 5].
- 8 Charité (DePuy Synthes, Raynham, MA, USA) and ProDisc-L (Centinel Spine, West Chester,
- 9 PA, USA) are two widely used articulating TDR systems designed to mimic the mechanical
- 10 function of the lumbar disc. Charité features an unconstrained design, while ProDisc-L employs
- a semi-constrained ball-and-socket configuration. While both devices preserve motion,
- biomechanical studies indicate that they do not fully replicate the stiffness and segmental
- mechanics of the native disc. These implants have been shown to significantly increase range of
- motion (RoM) and segmental lordosis compared to intact lumbar segments, particularly in
- 15 flexion-extension and axial rotation [6-8]. These mechanical differences may impact adjacent
- segment health and contribute to long-term complications.
- 17 Importantly, while articulating TDRs maintain or enhance motion, the flexibility they introduce
- 18 is not necessarily physiologic. The increased mobility and changes in contact mechanics suggest
- 19 a less stiff, more compliant segment than intended, especially in the absence of annular
- 20 structures. Though effective in reducing pain and restoring mobility, these devices may deviate
- 21 from the native disc's natural shock absorption and load-sharing characteristics, which are
- critical to spinal stability and function [6-8].

1 To address these shortcomings, viscoelastic total disc replacements (VTDRs) have been 2 engineered to mimic the shock absorption and flexural stiffness of the natural disc [9, 10]. Unlike 3 articulating ball-and-socket implants, VTDRs incorporate deformable polymer cores designed to 4 replicate the nonlinear stiffness of the native disc, stiffening progressively under increasing loads 5 while allowing controlled motion within physiological ranges. This viscoelastic behavior offers 6 the potential to restore not only RoM but also the native disc's capacity for shock absorption and 7 damping, thereby reducing stress on adjacent structures. 8 Despite these advancements, there remains limited published data directly comparing the 9 stiffness of a VTDR to that of the native lumbar disc under physiologic loading. To our 10 knowledge, this is the first in vitro study to quantify the stiffness behavior of a viscoelastic 11 lumbar disc across axial compression, flexion-extension, and axial rotation, and to compare these 12 values to reported benchmarks for healthy discs. 13 The objective of this study is to evaluate whether a VTDR can replicate the biomechanical 14 stiffness of the native lumbar disc in clinically relevant loading modes. By addressing this 15 knowledge gap, we aim to provide biomechanical validation for VTDRs as next-generation 16 implants capable of restoring natural spinal function more effectively than legacy articulating 17 designs. 18 19 2 Methods 20 Biomechanical testing was performed in accordance with applicable American Society for 21 Testing and Materials (ASTM) standards for total disc replacement (TDR) devices [11, 12]. In 22 line with the guidelines for evaluating functional performance, kinematics, and wear 23 characteristics of TDRs, functional failure was defined as any permanent deformation or wear

- that impairs the implant's ability to sustain normal loads or intended motion [13]. Mechanical
- 2 failure referred to material-related damage, such as fatigue cracks or bonding failure, that may or
- 3 may not result in functional impairment. Testing focused on the smallest available disc size (26
- 4 × 36 mm², 13 mm height, 12° lordotic angle) to represent the "worst-case scenario" for
- 5 mechanical durability. To capture the full performance range, range of motion (RoM) testing was
- also performed on the largest available size at the time $(28 \times 38 \text{ mm}^2, 16 \text{ mm height}, 12^{\circ} \text{ lordotic})$
- 7 angle). The AxioMed[®] Freedom Lumbar Disc (FLD) (AxioMed LLC, Burlington, MA, USA)
- 8 VTDR implants were preconditioned in phosphate-buffered saline (PBS) at 37 ± 3 °C for a
- 9 minimum of three days prior to testing, and all evaluations were conducted in a physiologic
- 10 temperature-controlled PBS environment. Each implant was mounted within custom steel
- fixtures and subjected to load using a servohydraulic testing system. An MTS 810 system (MTS,
- 12 Eden Prairie, MN, USA) was used for flexion-extension testing, while an INSTRON 8874
- 13 system (INSTRON, Norwood, MA, USA) was utilized for compression and torsion.
- RoM testing in axial compression and torsion was carried out on ten implants using quasi-static
- and cyclic loading protocols. Compressive loads ranged from 400 to 2000 N, while torsional
- loads were applied up to ±6 Nm. Key outcome measures included RoM, static stiffness
- 17 (calculated over the 400–600 N range for compression and at 4 Nm for torsion), dynamic
- stiffness (from a single cycle and averaged over the final five cycles), and hysteresis (recorded at
- 19 the 90th and 190th cycles for compression and torsion, respectively).
- For flexion-extension testing, ten implants were subjected to loads ranging from +8 Nm (flexion)
- 21 to -6 Nm (extension). Metrics included RoM, static and dynamic stiffness (from cycles 380 to
- 420), and hysteresis (measured at the 400th cycle). All data were captured under closed-loop
- 23 control to ensure consistency.

- 1 Static axial compression testing followed ASTM F2346 standards to assess construct stiffness
- 2 and failure thresholds. Five implants of the smallest size were tested under displacement control
- at a rate of 0.2 mm/s until reaching a 20,000 N force limit. Collected data included peak load,
- 4 displacement at peak load, physiologic-range stiffness, and mode of failure.
- 5 RoM and stiffness data from the viscoelastic disc were subsequently compared to published
- 6 cadaveric benchmarks of the native lumbar disc to evaluate the ability of the viscoelastic implant
- 7 to replicate natural biomechanical performance.

9

3 Results

- 10 3.1 Stiffness and Displacement
- 11 Under an axial compressive load of 2000 N, the axial displacement of the AxioMed[®] FLD
- ranged from 0.7 to 1.3 mm. The corresponding axial stiffness was measured between 1.55 and
- 13 3.48 kN/mm, which falls within or slightly exceeds the reported stiffness range of native lumbar
- discs (0.5–2.5 kN/mm) [14-18], indicating appropriate load-sharing capacity and resistance to
- 15 deformation under physiologic conditions.
- 16 3.2 Rotational Stiffness
- 17 In axial rotation, the FLD demonstrated stiffness values between 0.72 and 0.83 Nm/deg. This
- was lower than native lumbar disc stiffness, which typically ranges from 2.0 to 9.6 Nm/deg [16,
- 19 17, 19], suggesting the device allows greater rotational motion than the natural disc under similar
- 20 loading.
- 21 3.3 Flexion and Extension Stiffness
- 22 Flexion stiffness values for the FLD ranged from 1.4 to 2.12 Nm/deg, which overlaps with native
- 23 lumbar discs reported to range from 0.8 to 2.5 Nm/deg [17]. Extension stiffness ranged from 1.4

- to 2.14 Nm/deg, slightly below the native disc value of 2.1 Nm/deg [17], indicating comparable
- 2 resistance to motion in both flexion and extension planes.
- 3 3.4 Range of Motion (RoM)
- 4 RoM testing across all mechanical modes demonstrated that the viscoelastic disc maintains a
- 5 motion profile comparable to that of the human lumbar disc. No mechanical or functional
- 6 failures were observed in any of the tested implant sizes throughout ROM assessments.
- 7 3.5 Static Axial Compression
- 8 During static compression testing, stiffness increased nonlinearly with increasing load. All
- 9 devices remained structurally intact up to the 20,000 N load limit of the testing machine. The
- average displacement at peak load was 3.36 mm, and no device exhibited signs of mechanical or
- 11 functional compromise under high-load conditions.
- Table 1 summarizes the stiffness parameters between AxioMed[®] FLD and the native lumbar
- 13 disc.

15 4 Discussion

- 16 4.1 Brief Summary
- 17 This study evaluated the in vitro biomechanical performance of a AxioMed[®] VTDR device and
- compared its mechanical stiffness and RoM to that of the native human lumbar disc. While
- 19 earlier-generation TDRs often prioritized motion preservation without fully replicating
- 20 physiologic biomechanics, this study addresses the gap in comparative stiffness data by directly
- 21 measuring the mechanical response of a VTDR designed to simulate the natural disc's shock
- absorption and load distribution characteristics.

- 1 4.2 Key Findings
- 2 The VTDR device demonstrated axial compression stiffness values ranging from 1.55 to 3.48
- 3 kN/mm, consistent with or slightly exceeding native disc stiffness values reported in the
- 4 literature (0.5–2.5 kN/mm). These higher values, particularly in compression, the spine's primary
- 5 load-bearing direction, may confer improved implant stability and durability. In flexion and
- 6 extension, the VTDR stiffness (1.4–2.14 Nm/deg) closely matched native values (0.8–2.5
- 7 Nm/deg), further supporting its capacity to preserve physiologic motion. Although the device
- 8 showed lower stiffness in axial rotation (0.72–0.83 Nm/deg) than native discs (2.0–9.6 Nm/deg),
- 9 this resulted in increased RoM, which still fell within a functional, physiologic range. No
- 10 functional or mechanical failures were observed, and nonlinear load-displacement curves in
- static compression confirmed the presence of both neutral and elastic zones, replicating native
- disc mechanics.
- 13 4.3 Comparison with Similar Research
- 14 Previous TDR designs, particularly early-generation articulating devices, often failed to restore
- 15 the viscoelastic behavior of the intervertebral disc, resulting in excessive motion and low
- 16 resistance across the full RoM. In cadaveric and finite element studies, ProDisc-L has
- demonstrated up to a 91.4% increase in extension RoM and more than 150% increase in facet
- joint loading, indicating altered load transfer and segmental stiffness [8].
- 19 In contrast, the VTDR evaluated in this study reproduced both the compliant neutral zone and the
- 20 stiffening elastic zone seen in healthy discs, a feature rarely achieved in mechanical disc
- 21 replacements. A study at the Musculoskeletal Biomechanics Laboratory at Loyola University
- 22 Chicago Stritch School of Medicine illustrated how closely the FLD implant closely mirrored the
- 23 native disc at L4-5 in flexion-extension RoM loops (Figure 1).

1	4.4	Limitations

- 2 This study was limited to in vitro testing using standardized fixtures and physiologic loading
- 3 conditions. While this approach enables consistent comparison of device mechanics, it does not
- 4 account for biological factors such as bone-implant interface behavior, tissue remodeling, or
- 5 wear particle response. Additionally, cadaveric lumbar disc values used for comparison were
- 6 extracted from previously published literature rather than directly measured under identical
- 7 testing conditions.
- 8 4.5 Clinical Relevance
- 9 By replicating the stiffness and motion characteristics of the natural lumbar disc, this VTDR may
- offer advantages in load sharing, segmental stability, and shock absorption, critical elements for
- reducing adjacent segment degeneration and improving long-term outcomes. Its biomechanical
- profile supports its use in motion-preserving spine surgery as an alternative to fusion or legacy
- 13 TDRs, particularly in patients with high functional demands.
- 14 4.6 Implications for Further Research
- 15 Future studies should include cadaveric comparative testing under identical protocols, long-term
- 16 fatigue testing, and in vivo studies evaluating clinical outcomes, implant stability, and wear
- behavior. Additionally, analysis of kinematic coupling and segmental alignment over time will
- 18 be critical to validate this VTDR's functional durability and its effect on global spine
- 19 biomechanics.

21

5 Conclusion

- 22 This in vitro investigation is the first to directly evaluate and compare the stiffness of a
- 23 viscoelastic total disc replacement to published values for the native human lumbar disc. The

- 1 VTDR demonstrated physiologic stiffness and RoM in axial compression, flexion-extension, and
- 2 axial rotation. Its dual-zone mechanical behavior, characterized by a compliant neutral zone and
- 3 stiffening elastic zone, mirrors the natural stress-strain response of a healthy disc. These findings
- 4 support the potential of this VTDR to restore natural spinal function, offering a promising
- 5 alternative to both fusion and traditional TDR devices.

References

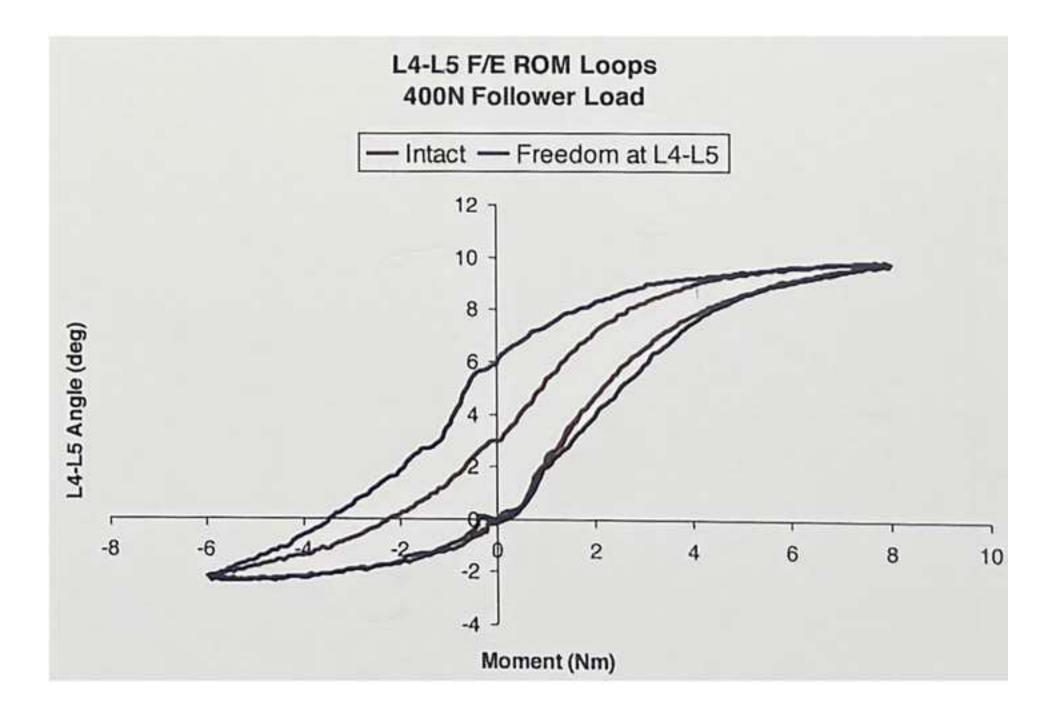
- 3 1. Blumenthal S, McAfee PC, Guyer RD, Hochschuler SH, Geisler FH, Holt RT, et al. A
- 4 prospective, randomized, multicenter Food and Drug Administration investigational device
- 5 exemptions study of lumbar total disc replacement with the CHARITE artificial disc versus
- lumbar fusion: part I: evaluation of clinical outcomes. Spine. 2005;30(14):1565-75; discussion
- 7 E387-91.
- 8 2. Rao MJ, Cao SS. Artificial total disc replacement versus fusion for lumbar degenerative
- 9 disc disease: a meta-analysis of randomized controlled trials. Arch Orthop Trauma Surg.
- 10 2014;134(2):149-58.
- 11 3. Li YZ, Sun P, Chen D, Tang L, Chen CH, Wu AM. Artificial Total Disc Replacement
- 12 Versus Fusion for Lumbar Degenerative Disc Disease: An Update Systematic Review and Meta-
- 13 Analysis. Turk Neurosurg. 2020;30(1):1-10.
- 14 4. Hsieh MK, Tai CL, Li YD, Lee DM, Lin CY, Tsai TT, et al. Finite element analysis of
- optimized novel additively manufactured non-articulating prostheses for cervical total disc
- replacement. Front Bioeng Biotechnol. 2023;11:1182265.
- 17 5. Jung T-G, Woo S-H, Park K-M, Jang J-W, Han D-W, Lee SJ. Biomechanical behavior of
- 18 two different cervical total disc replacement designs in relation of concavity of articular surfaces:
- 19 ProDisc-C® vs. Prestige-LP®. International Journal of Precision Engineering and
- 20 Manufacturing. 2013;14(5):819-24.
- 21 6. Wilke HJ, Schmidt R, Richter M, Schmoelz W, Reichel H, Cakir B. The role of
- prosthesis design on segmental biomechanics: semi-constrained versus unconstrained prostheses
- and anterior versus posterior centre of rotation. Eur Spine J. 2012;21 Suppl 5(Suppl 5):S577-84.
- 24 7. Demetropoulos CK, Sengupta DK, Knaub MA, Wiater BP, Abjornson C, Truumees E, et
- 25 al. Biomechanical evaluation of the kinematics of the cadaver lumbar spine following disc
- replacement with the ProDisc-L prosthesis. Spine. 2010;35(1):26-31.
- 27 8. Chen WM, Park C, Lee K, Lee S. In situ contact analysis of the prosthesis components of
- 28 Prodisc-L in lumbar spine following total disc replacement. Spine. 2009;34(20):E716-23.
- 29 9. Lazennec JY. Lumbar and cervical viscoelastic disc replacement: Concepts and current
- 30 experience. World J Orthop. 2020;11(8):345-56.
- 31 10. Lazennec JY, Rakover JP, Rousseau MA. Five-year follow-up of clinical and radiological
- 32 outcomes of LP-ESP elastomeric lumbar total disc replacement in active patients. The spine
- 33 journal : official journal of the North American Spine Society. 2019;19(2):218-24.
- 34 11. F2346 AS. "Standard Test Methods for Static and Dynamic Characterization of Spinal
- 35 Artificial Discs," ASTM International, West Conshohocken, PA. 2005.
- 36 12. F2423 AS. "Standard Guide for Functional, Kinematic, and Wear Assessment of Total
- Disc Prostheses," ASTM International, West Conshohocken, PA. 2005.
- 38 13. Benzel EC, Lieberman IH, Ross ER, Linovitz RJ, Kuras J, Zimmers K. Mechanical
- 39 Characterization of a Viscoelastic Disc for Lumbar Total Disc Replacement. J Med Devices.
- 40 2011;5(1):011005(1)-(7).
- 41 14. Berkson MH, Nachemson A, Schultz AB. Mechanical Properties of Human Lumbar
- 42 Spine Motion Segments—Part II: Responses in Compression and Shear; Influence of Gross
- 43 Morphology. J Biomech Eng. 1979;101(1):53-7.
- 44 15. Tencer AF, M. AA, D.L. B. Some Static Mechanical Properties of the Lumbar
- 45 Intervertebral Joint, Intact and Injured. J Biomech Eng. 1982;104(3):193-201.

- 1 16. White AA, Panjabi MM. Clinical Biomechanics of the Spine. 2nd Edition: Lippincott
- Williams and Wilkins, Philadelphia.; 1990.
- 3 17. Eijkelkamp MF, van Donkelaar CC, Veldhuizen AG, van Horn JR, Huyghe JM,
- 4 Verkerke GJ. Requirements for an artificial intervertebral disc. The International Journal of
- 5 Artificial Organs. 2001;24(5):311-21.

- 6 18. Li S, Patwardhan AG, Amirouche FM, Havey R, Meade KP. Limitations of the standard
- 7 linear solid model of intervertebral discs subject to prolonged loading and low-frequency
- 8 vibration in axial compression. J Biomech. 1995;28(7):779-90.
- 9 19. Schultz AB, Warwick DN, Berkson MH, Nachemson AL. Mechanical Properties of
- 10 Human Lumbar Spine Motion Segments—Part I: Responses in Flexion, Extension, Lateral
- 11 Bending, and Torsion. J Biomech Eng. 1979;101(1):46-52.

1 Figure Legend

- 2 Figure 1: Moment versus Angel of the Freedom Lumbar Disc Compared To the Native Lumbar
- 3 Disc.



1 Table 1 summarizes the stiffness parameters between AxioMed FLD and the native lumbar disc.

Parameter	AxioMed FLD	Native Lumbar Disc
Axial Compression Stiffness (kN/mm)	1.55-3.48	0.5-2.5
Axial Rotational Stiffness (Nm/Deg)	0.72-0.83	2.0-9.6
Flexion Stiffness (Nm/deg)	1.4-2.12	0.8-2.5
Extension Stiffness (Nm/deg)	1.4-2.14	2.1